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Stereotactic Body Radiotherapy for Lung Lesions using Multiple Phase 3D-CT Based on the Analysis of Radiobiological Parameters

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| ARTICLE INFO | ABSTRACT |
|---|--|
| <i>Article type:</i> Original Article | Introduction: Planning target volume (PTV) is generated from internal treatment volume (ITV) using four- dimensional computed tomography (4D-CT) for enhanced therapeutic gain in the stereotactic body |
| Article history: Received: Sep24, 2018 Accepted: Dec01, 2018 | radiotherapy for lung lesions (SBRT-Lung). This study aimed to propose a strategy to generate ITV on multiple-phase 3D-CT and enhance therapeutic gain in SBRT-Lung. <i>Material and Methods:</i> This study was conducted on 6 peripherally located and 5 centrally located lung lesions suitable for SBRT. The PTV was delineated based on 3D-CT datasets acquired at three different phases of respiratory motion. The prescribed dose of 50 Gy in 5 fractions was delivered using RapidArc |
| <i>Keywords:</i> SBRT-Lung Radiobiology Volumetric-Modulated Arc | technique. The therapeutic-gain was compared based on tumor control probability (TCP) and normal tissue complication probability (NTCP) against a multicenter trial, which uses single-phase 3D-CT for PTV delineation. The TCP and NTCP were calculated by Poisson's linear-quadratic and Lyman-Kutcher-Burman models, respectively. |
| Therapy | Results: Regarding the multicentre trial, the PTVs were maximally reduced to 42% and 57% among the 6 peripherally and 5 centrally located lung lesions, respectively. In peripheral lung lesions, TCP was significantly enhanced to 0.6% for long-term (>5years) local control (P <0.05), and NTCP was significantly reduced in pneumonitis (Grade≥II) of lung (0.2%; P <0.05). In central lung lesions, TCP was insignificantly enhanced; however, NTCPs were maximally reduced for cartilage necrosis in trachea (35%) and myelitis in spinal cord (19%). Conclusion: The proposed strategy reduced the complications for normal tissues and enhanced therapeutic |
| | gain. The successful clinical outcomes validated our hypothesis in short-term (6-12 months), and we are currently testing the long-term efficacy. |

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Introduction

Stereotactic body radiotherapy (SBRT) delivers an ablative radiation dose to tumors that are located at inoperable sites and are closely aligned with normal organs. The SBRT can lead to the non-invasive achievement of the high rates of local control for lung lesions (up to 90%); therefore, SBRT is widely considered an effective alternative to lobectomy for early-stage non-small cell lung cancer (stage I) [1-4]. Advanced technologies used for radiotherapy reduce toxicity to normal tissue and enhance the quality of post-treatment life [5-7]. The efficiency of SBRT in delivering an ablative dose to the tumor relies on the generation of a robust planning target volume (PTV) from the gross tumor volume (GTV) using threedimensional computed tomography (3D-CT) images.

Respiratory motion is a major challenge for the delineation of a robust PTV in lung-SBRT. Internal treatment volume (ITV) is the volume within which

the tumor oscillates during a particular breathing pattern. The ITV is generated by combining GTV and internal margin (IM). The IM is the margin for drift of tumor during respiratory motion [8]. The IM has been derived by different tumor tracking systems, such as fluoroscopy, orthogonal portal image, dynamic magnetic resonance image, multiple-phase 3D-CT, and four-dimensional computed tomography (4D-CT). During respiratory motion, the lung lesion oscillates more in craniocaudal direction than in transversal direction [9-14]. The PTV has been widely delineated either by 4D-CT or 3D-CT protocol in a multicenter trial for lung-SBRT [15]. The trial recommends the delineation of PTV either by expanding ITV with 5-mm isotropic margin on 4D-CT [16] or expanding the GTV with 5-mm margin in the axial direction and 10-mm margin in the longitudinal direction on 3D-CT [3].

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The delineation of PTV margins from ITV is more robust and reproducible in lung-SBRT. As a result, PTVs are preferably delineated with the 4D-CT protocol than 3D-CT protocol in multicenter trials. The delineation of PTV for lung-SBRT by expanding GTV with additional margins on 3D-CT yields larger treatment volume up to two times more than expanding ITV with additional margins either on 4D-CT or multiple-phase 3D-CT [17-20]. Subsequently, this study was motivated to propose a strategy to delineate PTVs from ITVs on multiple-phase 3D-CT for lung-SBRT. The evaluation of tumor response to a treatment regimen is based on 'Response Evaluation Criteria in Solid Tumors' (RECIST) [21].

The clinical outcome depends on various prognostic factors in tandem to SBRT-Lung. The analyses of radiobiological parameters reveal the quality of radiotherapy delivered through different PTV delineation protocols for lung-SBRT. Tumor control probability (TCP) and normal tissue complication probability (NTCP) are the two radiobiological parameters available for evaluating the efficiency of PTV delineation protocols. Various radiobiological models of cell survival curves have been used for a high-dose-hypo-fractionated scheme of SBRT [22-27]. Poisson's linear-quadratic (PLQ) cell survival model has been used in conventional 2-Gy/fraction dose regimens (EQD₂) and recent studies have supported their applicability in estimating the TCP for SBRT-Lung [28-30].

In the current study, PLQ and Lyman-Kutcher-Burman (LKB) models were employed to calculate the relative efficiencies of different radiotherapy plans. The purpose of this study was to investigate the impact of PTV delineation based on radiobiological parameters in peripherally and centrally located lung lesions for SBRT-Lung patients. The researchers hypothetically tested the radiobiological parameters for radio-therapeutic gain with a change in PTV delineation strategies. This comparative study reported (i) multiple-phase 3D dose calculation in order to account the respiratory motion and observed variations in radiobiological parameters, (ii) normal tissue complications due to a generous planning target volume, and (iii) post-treatment set-up errors in terms of observed variations in radiobiological parameters.

Materials and Methods

Treatment Simulation and Target Delineation

This study was conducted on 6 peripherally located and 5 centrally located lung lesions suitable for SBRT (Table1). 7 patients were immobilized on a Vac-Lok cushion with indexing features (M/s.Civco, Coralville, IA, USA) using a pneumatic abdominal compression system, as described by Lovelock et al. [31]. The pneumatic abdominal compression system used in this study consisted of a commercially available sphygmomanometer (M/s. WelchAllyn®, Skaneateles Falls, NY, USA) and nylon strap with a VelcroTM fastener. The CT datasets were acquired using a helical CT machine (Biograph; M/s. Siemens Healthcare, Erlangen, Germany).

Lesions located within 2-cm from the proximal bronchial tree are considered as centrally located and others are categorized as peripherally located lung lesions.

Patients were trained to perform shallow breathing, and baseline CT datasets for planning purposes were acquired at random breathing phase. More CT datasets with deep inspiration breath-hold (DIBH) and deep expiration breath-hold (DEBH) phases were acquired for evaluating IMs. The strategy was approved by the Ethics Committee of the Cancer Care of Jaypee Hospital, Noida, India. Baseline CT datasets were considered for GTV delineation. The IMs for accommodating the movements of GTV during respiratory motions were taken from CT datasets acquired at DIBH and DEBH, by which ITV was subsequently delineated. The ITV was further expanded with 3-mm margin to generate the PTV on baseline CT datasets. Critical organs, such as the lungs, ribs, esophagus, trachea, spinal cord, and heart, were also contoured on the baseline CT datasets.

Treatment Planning

The SBRT-Lung was delivered on TrueBeamSTx platform Linac (Varian Medical Systems, Palo Alto, CA) equipped with HD120TM MLC. Treatments were planned using the Eclipse External Beam Planning (Version 13.0.33). The prescription dose to PTV was 50 Gy delivered in 5 fractions using RapidArc technique. The RapidArc plan consisted of 2 co-planar treatment arcs (first in a clockwise direction - 181° to 179° and second in a counter-clockwise direction - 179° to 181°).

| | radier. Summary of distribution of lung lesions in patients | | | | | | | | | |
|--------------|---|--------------|---------|----|------------|---------|--|--|--|--|
| Patient No. | Histology | Tumor Stage | No. | of | Location | | | | | |
| I attent NO. | Histology | Tunior Stage | Lesions | | Peripheral | Central | | | | |
| 1 | Intraductal Carcinoma | IV | 1 | | 1 | - | | | | |
| 2 | Squamous Cell Carcinoma | IIB | 1 | | - | 1 | | | | |
| 3 | Hepatocellular Carcinoma | IV | 2 | | 1 | 1 | | | | |
| 4 | Squamous Cell Carcinoma | IA | 1 | | - | 1 | | | | |
| 5 | Squamous Cell Carcinoma | IVB | 1 | | 1 | - | | | | |
| 6 | Adenocarcinoma | IVA | 2 | | 2 | - | | | | |
| 7 | Adenocarcinoma | IVA | 3 | | 1 | 2 | | | | |
| Total | | | 11 | | 6 | 5 | | | | |

Table 1 Summary of distribution of lung lesions in patients

| Structure | Endpoint/Stage | Biological Model | D ₅₀ (Gy) | α/β (Gy) | γ | S | n | m |
|-------------|-------------------------------------|---------------------|-------------------------|-------------|-----|------|------|----------|
| GTV | 36-month local control | PLQ | 42.3 | 10 | 0.9 | - | - | - |
| & ITV | Long term (> 5 years) local control | PLQ | 49.2 | 10 | 1 | - | - | - |
| Lung | Pnuemonitis, Grade - ≥II | LKB | 30.8 | 3 | - | - | 0.99 | 0.3 7 |
| Rib | Pathologic fracture | PLQ | 65.0 | 3 | 2.3 | 1 | - | - |
| Esophagus | Esophagitis,Grade - \geq II | LKB | 51.0 | 10 | - | - | 0.44 | 0.3 2 |
| Trachea | Cartilage necrosis | PLQ | 78.8 | 3 | 4.8 | 0.66 | - | - |
| Spinal Cord | Necrotic Myelitis | PLQ | 68.6 | 3 | 1.9 | 4 | - | - |
| Heart | Pericarditis | PLQ | 49.2 | 3 | 3 | 0.2 | - | - |

Table 2. Summary of radiobiological cost functions for the calculations of tumor control probability and normal tissue complication probability

GTV: gross tumor volume, ITV: internal target volume, PLQ: Poisson linear-quadratic model [35-37], LKB: Lyman-Kutcher-Burman model [38-39], D_{50} rate of control and complication at 50% for TCP and NTCP, respectively, α/β : dose at which linear and quadratic components of cell killing are equal, γ : normalized dose-response gradient at maximum, s: parameter to account relative seriality of an organ's internal organization, m: slope of the cell survival curve, n: parameter to account irradiated volume of an organ

Progressive resolution optimizer (Version 13.0.26) was utilized for RapidArc optimization, and the jaws were set for tracking PTV by enabling the "Jaw Tracking" option. Acuros External Beam (Version 13.0.26) was employed to compute volumetric doses to heterogeneous medium with 1-mm grid resolution [32]. Patient's treatment set-up was verified by On-Board Imager[®] (OBI) and accurately repositioned on PerfectPitchTM couch with 6 degrees of freedom. Patients were reminded to perform shallow breathing during image verification and treatment. Target localization and set-up verification before and after treatment were accomplished based on cone-beam computed-tomography acquired by OBI and baseline CT datasets. The target localization and set-up verification procedures for SBRT-Lung were performed as described by other medical professionals [33,34].

Comparison with Multicenter Trial

The PTV delineation protocols of radiation therapy oncology groups (RTOG) multicenter trial- 0915 [15] was considered to evaluate the efficiency of the proposed strategy to delineate PTV using multiple-phase 3D-CT in SBRT-Lung. The protocol [15] for PTV delineation in SBRT-Lung (i.e., GTV with an additional margin of 5-mm in transversal and 10-mm in longitudinal planes from single-phase 3D-CT) was used to generate standard PTV (PTV2), which was compared with the efficiency of the proposed PTV (PTV1) delineated with multiple-phase 3D-CT strategy. Consort diagram for this comparison study is displayed in Figure 1. The original plan delivered to the patient was considered as the proposed plan (PP). The RapidArc identical beam arrangement was planned with retrospectively to deliver the prescribed dose to standard PTV (PTV2) and renormalized identically to mean dose received by ITV in PP. The results of the obtained plan were considered the standard plan (SP) and was compared with the PP.

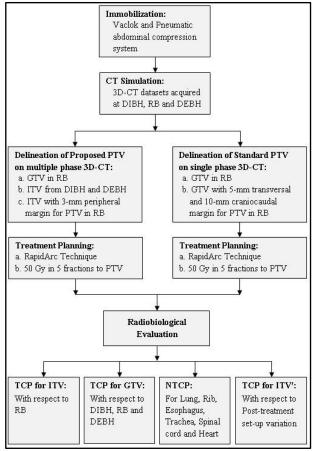


Figure 1. Consort diagram for the comparative study of strategies used for delineating planning target volumes from 3D-CT and comparing radiobiological parameters during respiratory movements and post-treatment set-up variations

Radiobiological Analysis

Radiobiological parameters, such as TCP and NTCP, were evaluated based on the dose-volume histogram of both the SBRT-Lung plans (PP and SP). Radiobiological estimates were evaluated in Biological Evaluation software (M/s. Varian Medical Systems) using PLQ and LKB models. The PLQ model was based on cell survival model with Poisson distribution, whereas the LKB model was based on cell survival model with a standard normal distribution. Table2



tabulates the cost functions of cell survival model used for the evaluation of TCP and NTCP [32, 35-39]. The radiobiological parameters of the both plans were evaluated in the aspects of tumor displacement and tissue heterogeneity during the respiratory movements and reproducibility of dose delivery beyond treatment set-up variations. The effectiveness of PTV delineation protocols was analyzed for the enhancement of TCP and reduction of NTCP using two-tailed paired sample t-test. The difference between PP and SP was considered significant (P<0.05).

Results

The GTVs, the resultant ITVs, and PTVs were within the range of 2-22 cm³ (Table3). Internal margins for ITV due to respiratory movements of GTV varied with respect to tumor size and location (Table3). The

IMs were found negligible for centrally located lung lesions but enlarged to more than 120% of the GTV for peripherally located lung lesions. The proposed PTV was found smaller than the standard PTV up to 42-57% in peripherally and centrally located lung lesions, respectively. As the standard PTVs were delineated solely from GTV, it was independent of ITV. Consequently, the inclusion of ITV in standard PTV varied from 100% to 79% in peripherally located lung lesions. Due to negligible IMs in each centrally located lung lesion, 100% of ITVs were included in the entire standard PTVs. This variation in the inclusion of ITVs within proposed and standard PTVs altered the dose distribution in ITV (Figure 2). As a result, the tumor control probability varied with dose distribution in the treatment target at different breathing phases(Table4).

| Table 3. Characteristics of treatment volume | es in peripherally a | and centrally located lesions |
|--|----------------------|-------------------------------|
|--|----------------------|-------------------------------|

| S.No. | GTV (cm ³) | ITV (cm ³) | PTV1 (cm ³) | PTV2 (cm ³) | ITV∩PTV2 (cm ³) | Enlargement of Internal Margins (%) | Reduction of PTV (%) | Inclusion of ITV within PTV2 (%) |
|---------|---------------------------|---------------------------|----------------------------|----------------------------|--------------------------------|---|----------------------|-------------------------------------|
| Periphe | rally Located | Lesions | | | | | | |
| 1 | 1.60 | 2.50 | 6.50 | 11.30 | 2.20 | 56.25 | 42.48 | 88.00 |
| 2 | 2.40 | 4.70 | 11.70 | 15.40 | 3.70 | 95.83 | 24.03 | 78.72 |
| 3 | 3.00 | 4.50 | 10.50 | 16.90 | 4.50 | 50.00 | 37.87 | 100.00 |
| 4 | 3.20 | 5.00 | 12.00 | 19.30 | 5.00 | 56.25 | 37.82 | 100.00 |
| 5 | 5.20 | 11.60 | 24.70 | 24.30 | 11.30 | 123.08 | -1.65 | 97.41 |
| 6 | 11.20 | 17.40 | 34.10 | 43.60 | 17.00 | 55.36 | 21.79 | 97.70 |
| Mean | 4.43±3.22 | 7.62 ± 5.21 | 16.58±9.63 | 21.80±10.51 | 7.28 ± 5.20 | 72.79±27.17 | 27.06±14.90 | 93.64±7.81 |
| Central | ly Located Les | sions | | | | | | |
| 1 | 2.30 | 2.30 | 8.50 | 16.80 | 2.30 | 0.00 | 49.40 | 100.00 |
| 2 | 2.40 | 2.40 | 6.90 | 16.00 | 2.40 | 0.00 | 56.88 | 100.00 |
| 3 | 4.30 | 4.30 | 13.40 | 24.10 | 4.30 | 0.00 | 44.40 | 100.00 |
| 4 | 5.50 | 5.50 | 13.00 | 28.60 | 5.50 | 0.00 | 54.55 | 100.00 |
| 5 | 22.20 | 22.20 | 38.60 | 63.10 | 22.20 | 0.00 | 38.83 | 100.00 |
| Mean | 7.34±7.53 | 7.34±7.53 | 16.08 ± 11.54 | 29.72±17.33 | 7.34±7.53 | 0.00 ± 0.00 | 48.81±6.59 | 100.00±0.00 |

GTV: gross tumor volume, ITV: internal treatment volume, PTV1: proposed planning target volume, PTV2: standard planning target volume, ITV∩PTV2 – ITV intersecting with standard PTV

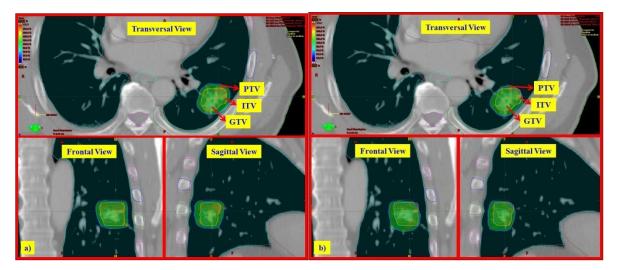


Figure 2.Variation of dose distribution in ITV due to strategies for PTV delineation (a) proposed strategy to delineate from ITV using multiplephase 3D-CT (b) standard strategy to delineate from GTV using single

| | | 2 | 1 | 5 | | 1 1 | | 5 | | |
|----------------------|----------------------|-------|--------------------|------------------|------------------|---------|------------------|------------------|---------|--|
| Tractment | | | Dreathing | Peripheral | | | Central | | | |
| Treatment Volumes | End Stage | | Breathing Phase | Proposed Plan | Standard Plan | P-value | Proposed Plan | Standard Plan | P-value | |
| ITV | 36-Month Control | Local | RB | 95.79±0.09 | 95.61±0.13 | 0.007 | 95.77±0.06 | 95.76±0.06 | 0.589 | |
| | Long Term Control | Local | RB | 92.52±0.15 | 92.24±0.21 | 0.005 | 92.50±0.10 | 92.48±0.09 | 0.506 | |
| | | | RB | 95.77±0.12 | 95.70±0.12 | 0.193 | 95.77±0.06 | 95.76±0.06 | 0.589 | |
| | 36-Month | Local | DIBH | 96.21±0.55 | 96.05±0.48 | 0.016 | 95.78±0.06 | 95.77±0.06 | 0.655 | |
| | Control | | DEBH | 96.09±0.25 | 95.97±0.20 | 0.203 | 95.77±0.06 | 95.76±0.05 | 0.546 | |
| GTV | | | Combined | 96.02±0.40 | 95.91±0.34 | 0.003 | 95.77±0.06 | 95.76±0.06 | 0.291 | |
| GIV | | | RB | 92.49±0.20 | 92.37±0.19 | 0.187 | 92.50±0.10 | 92.48±0.09 | 0.506 | |
| | Long Term | Local | DIBH | 93.24±0.92 | 92.97±0.80 | 0.017 | 92.50±0.09 | 92.48±0.10 | 0.560 | |
| | Control | | DEBH | 93.03±0.42 | 92.83±0.33 | 0.205 | 92.50±0.10 | 92.48±0.08 | 0.483 | |
| | | | Combined | 92.92±0.67 | 92.72±0.57 | 0.003 | 92.50±0.10 | 92.48±0.09 | 0.193 | |
| ITV' | 36-Month Control | Local | RB | 95.79±0.10 | 95.61±0.14 | < 0.001 | 95.76±0.08 | 95.75±0.06 | 0.071 | |
| | Long Term Control | Local | RB | 92.52±0.17 | 92.24±0.23 | < 0.001 | 92.49±0.13 | 92.46±0.11 | 0.012 | |

Table 4. Summary of tumor control probability for treatment volumes in peripherally and centrally located lesions

ITV: tumor control probability calculated for internal target volume in RB phase, GTV: tumor control probability calculated for gross tumor volume during RB, DIBH, and DEBH breathing phases Combined - Mean value of RB, DIBH, and DEBH, ITV': tumor control probability calculated for internal treatment volume in RB phase with respect to post-treatment set-up variation of patients. RB: shallow breathing random phase, DIBH: deep inspiration breath-hold, DEBH: deep expiration breath-hold. TCP values are represented in percentage.

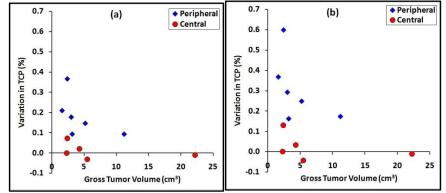


Figure3.Variation in TCP on the proposed plans with respect to standard plans for (a) 36-month local control and (b) long-term local control in peripherally and centrally located lung lesions.

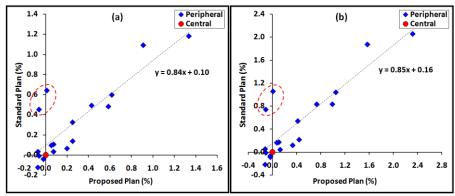


Figure4.Variation in TCP due to respiratory movements on the proposed plans and corresponding standard plans for (a) 36-month local control and (b) long-term local control in peripherally and centrally located lung lesion

Thirty-Six Month Local Control

Proposed and standard plans yielded TCP (36-month local control) of $95.79\pm0.09\%$ and $95.61\pm0.13\%$, respectively, with identical mean doses delivered to ITV in peripherally located lung lesions (Table4). In centrally located lung lesions, TCP of $95.77\pm0.06\%$ and $95.76\pm0.06\%$ were yielded by PP and SP, respectively.

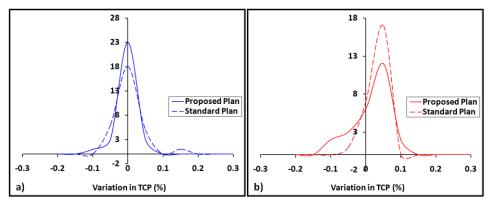
Variations in TCP (ITV) between PP and SP were displayed with respect to tumor size and location in Figure 3 (a). As the ITV was encompassed by the proposed PTV, PP enhanced the TCP significantly up to 0.35% in peripherally located lung lesions (P<0.05). However, in centrally located lung lesions, the difference in TCP between PP and SP was insignificant.

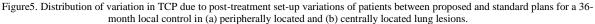


| | | Perip | heral | P-value | Cei | P-value | | |
|----------------|-------------------------------|-----------------|-------------------------|--------------|------------------|------------------|--------------|--|
| Organs | End Stage | Proposed Plan | osed Plan Standard Plan | | Proposed Plan | Standard Plan | (n) | |
| Lung | Pnuemonitis,Grade - \geq II | 0.87±0.29 | 1.00±0.25 | 0.001 (6) | 0.67±0.26 | 0.96±0.51 | 0.079 (5) | |
| Rib | Pathologic fracture | 29.50±27.20 | 36.98±32.64 | 0.064 (7) | 25.28±18.3 7 | 36.47±26.83 | 0.117 (4) | |
| Esophagus | Esophagitis,Grade - \geq II | 0.24±0.08 | 0.25±0.10 | 0.402 (5) | 1.10±0.88 | 2.40±2.30 | 0.142 (5) | |
| Trachea | Cartilage necrosis | 0.00 ± 0.00 | 0.00 ± 0.00 | (6) | 26.74±1.99 | 61.30±11.33 | (2) | |
| Spinal Cord | Necrotic Myelitis | 0.00 ± 0.00 | 0.00 ± 0.00 | (6) | 7.82±0.00 | 26.76±0.00 | (1) | |
| Heart | Pericarditis | 0.00 ± 0.00 | 0.00 ± 0.00 | (6) | 0.00 ± 0.00 | 0.00 ± 0.00 | (5) | |

Table5.Summary of Normal Tissue Complication Probability for critical organs in peripherally and centrally located lesions

NTCP values are represented in percentage. n: the sample size, (n-1): degree of freedom





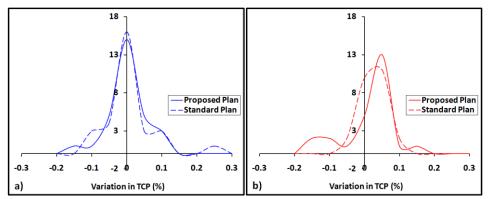


Figure6. Distribution of variation in TCP due to post-treatment set-up variations of patients between proposed and standard plans for long-term local control in (a) peripherally located and (b) centrally located lung lesions.

Long Term (> Five years) Local Control

In peripherally located lung lesions, TCP (Long term local control) remained at $92.52\pm0.15\%$ and $92.24\pm0.21\%$ for PP and SP, respectively (Table4). In centrally located lung lesions, TCP was $92.50\pm0.10\%$ and $92.48\pm0.09\%$ for PP and SP, respectively. Likewise, in 36-month local control, PP significantly enhanced the TCP for long term local control (0.6%) in peripherally located lung lesions, whereas the difference in TCP between PP and SP was insignificant in centrally located lesions, (Figure 3[b]).

Multiple Phase 3D-Dose Calculation

The multicenter trial urges that the GTV should be confined within PTV at any instance [15]. Accordingly, TCP was calculated through dose distribution in GTVs at DIBH, RB, and DEBH phases from PP and SP. The TCP varied based on the movement of GTV during respiratory motion due to the heterogeneous density of lung and tumor tissues (Table4). Compared to TCP of ITV, the TCP of GTV was enhanced in all the phases of respiratory motions during the treatment of peripherally located lesions (Figure 4). Meanwhile, in centrally located lung lesions, the negligible movement of GTV during respiratory motion led to an insignificant difference between TCP of GTV and ITV. The TCPs were enhanced up to 1.2% and 2.0% during the respiratory motion for 36-month and long-term local control, respectively.

Normal Tissue Complication Probability

Normal tissue complication probabilities were calculated for different critical organs with specific endpoint/stage (Table5). In peripherally located lung lesions, NTCP were significantly low for the lungs; however, this level was not significantly low for other organs (rib and esophagus) with PP than the SP (P<0.05). However, NTCPs remained null for the trachea, spinal cord, and heart in both plans. In centrally located lung lesions, there were significantly lower levels in PP with regard to NTCPs for all the critical organs. However, NTCPs were higher with SP and up to 35% for cartilage necrosis in the trachea and 19% for myelitis in the spinal cord.

Clinical Outcome

The obtained results of the current study revealed that 7 patients of this study had 11 lung lesions, out of which 6 were peripherally located and 5 were centrally located. The post-treatment clinical follow-ups of the patients who underwent SBRT-Lung were conducted after 6 and 12 months after treatment. The 12-month follow-ups revealed no residual tumors in the treatment beds of any patient as per the RECIST. A patient treated for a peripheral lung lesion reported that he experienced asymptomatic lung pneumonitis (ALP) in the dose falloff region during his 6-month follow-up. However, his ALP decreased extensively over the next six months.

Discussion

The analysis of radiobiological parameters of TCP and NTCP revealed the significance of IMs in SBRT-Lung in the context of clinical utility. In this study, the IMs that accounted for tumor dislocations due to respiratory motions were derived using multiple-phase 3D-CT. In a clinical case study, the radiobiological utility of our institutional SBRT-lung protocol had a better performance with respect to several aspects than the multicenter trials based on 3D-CT [32].

The enhancement of toxicity to normal tissue due to the negligence of internal margins in SBRT-lung was discussed earlier [40, 41]. The IM estimations that were derived using multiphase 3D-CT or 4D-CT rendered a 50% reduction of PTV [17, 42-44] than conventional estimates [3]. In the current study, the ITV was identical to the GTV in centrally located lung lesions (Table3), leading to a 57% reduction of PTV than PTVs that were delineated using 3D-CT in multicenter trials [3, 15].

Furthermore, in the current study, the reduction in PTV levels results in the decrease of NTCP for the trachea from 61.30% of the standard plans to 26.74%. Correspondingly, the NTCP for the spinal cord was reduced to 7.82% from the standard plan value of 26.76% (Table5). Similarly, the NTCP for Grades \geq II

lung pneumonitis was significantly reduced in SBRT for peripherally located lung lesions because IMs were accounted for the delineated PTV. Excessive toxicities were predicted in our radiobiological analysis due to the omission of internal margins of standard PTV in the centrally located lesions. The current results were in agreement with the earlier observations of clinically excessive toxicities [40, 41, 45]. Excessive toxicities have been related to the biologically effective dose (BED) (their trial \geq 180 Gy) [45], although the negligence of IMs was indeed a prognostic factor for NTCP and excessive toxicities.

In this study, the BED was 100 Gy (50 Gy in 5 fractions), which yielded TCP of ~95% and 92% for 36-month and long term local control, respectively. The BED of 100 Gy has been widely acknowledged to be sufficient for long-term local control [35, 46-49]. Guckenberger observed that the TCP was ~90% for a BED of 100 Gy with 4D-dose calculations, whereas the BED was 80 Gy with 3D-dose calculations [35]. Typical 4D-dose calculations indicated variations in absorbed dose due to MLC interplay effects, tumor dislocation during respiratory movements, and patient set-up variations during treatment.

Variations in prescribed dose delivery due to MLC interplay effects have been found to be negligible in SBRTs [50-54], particularly in SBRT-lung [51]. Therefore, the interplay effect was not emphasized in this report. The study was a thorough investigation of variations in dose distribution and the resultant TCPs due to tumor dislocation during respiratory movements and patient set-up variations during treatment. The variation in the TCP (GTV) was calculated as a surrogate for tumor dislocation during respiratory movements. When the TCP (GTV) was calculated at DIBH and DEBH phases, the volume of lung tissues in ITV was replaced by a relatively high-density GTV, and application of the Acuros algorithm increased the dose to GTV. As a result, the TCP (GTV) was enhanced during respiratory movements, compared to the TCP (ITV) on baseline CT dataset. The TCP (GTV) enhancement was proportionate in the both PTV delineation strategies, except when the ITV extended beyond the standard PTV (encircled in Figure 4). As ITV was identical to GTV in centrally located lung lesions, the TCP (GTV and ITV) remained unaltered during respiratory movements.

Variations in the TCP (ITV') with respect to patient set-up variations during treatment were retrospectively computed according to the patient data. The TCPs were remained consistent within $\pm 0.3\%$ both in proposed and standard plans (figure 5 and 6). The PTV generated with a 3-mm margin from ITV on 4D-CT rendered good local control with lesser toxicities [42, 43, 55]. Similarly, in the current study, a 3-mm PTV margin from the ITV reduced the NTCP and improved the TCP. Consequently, an optimum therapeutic ratio was obtained by the proposed PTV margin in SBRT-Lung with 3D-CT acquired at multiple phases of respiratory movements.

Conclusion

During SBRT-Lung, the reproducible positioning of the tumor that is computed on the basis of baseline CT datasets remains vital in delineating the treatment volume. This is more likely to be achieved with tumor motion mitigation accessories. The estimation of IM in PTV assured the reliability of delineated treatment volume and reduced complications due to the irradiation of surrounding normal tissues. The PTV margin derived from ITV, reduced the NTCP both in centrally and peripherally located lung lesions; however, it enhanced TCP in peripherally located lung lesions for the given BED (100 Gy). The current study demonstrates that the strategy of delineating treatment volume using multiplephase 3D-CT has the potential to reduce complications in irradiated normal tissues and enhance therapeutic gains in SBRT-Lung. The proposed strategy has the potential to yield comparable lesser toxicities as in 4D-CT strategy.

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